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Device in connection with pacersTechnical field of the invention.

The present invention relates to pacemaker housings and more particularly to those parts of the housing intended for connection to the electrode leads.

Background of the invention.

Implantable pacers normally comprise a pacemaker housing (also called can) containing electronic circuitry and a unit for electric power as well as different electrodes which are connected to the interior parts in the pacemaker housing and which are to be implanted in or in the vicinity of the heart. The electrodes are connected to the pacemaker by means of leads. The internal parts of the pacers have to be well protected against the internal environment, especially the body fluids in the body for a long period of time, which places strict requirements on all entries into the interior of the can and especially on the connections of the leads to the housing. At the same time it should be possible to disconnect the pacemaker from the implanted leads for replacement or servicing of the pacemaker. The connective parts of the pacemaker and the leads have largely been standardized so as to encompass a relatively deep female socket comprising a number of contact surfaces whereas the leads are provided with a male part comprising one or several corresponding peripheral, generally circular contact surfaces.

At present the connective part of the pacemaker housing containing the female socket is made of a transparent material, normally of epoxy resin, which is molded onto the housing and onto contacts extending outwardly from the housing. The male part of the leads is normally locked by means of set screws, although other fastening means have been envisaged. The positioning and alignment of the different contact surfaces and of the fastening means or metallic threads for the set screws prior to the molding of

the connective part is however complicated and the delay in the manufacturing process incurred by the curing of the epoxy resin is considerable.

- 5 It would thus be desirable if the molding procedure could be dispensed with.

It has been discussed that these complexities could be avoided by designing the pacemaker with a socket located inside  
10 the metal housing. To our knowledge this kind of sockets, sometimes termed "black holes", are not used at present.

US-A-4,934,366 and US-A-5,324,311, both of which are incorporated by reference, describe two interior sockets or  
15 black holes for pacemakers. Both designs comprise a tubular member consisting of a number of longitudinally alternating sections made of metal respectively of insulating ceramics. An end section of metal can be welded or bonded to an opening in the pacemaker housing by means of a flange. The use  
20 of different materials however set high standards in regard of precision and durability of the component parts as well as on the assembly procedure thereof. This is especially important since the interior sockets must meet very high standards regarding the integrity of the interior of the  
25 pacemaker housing during long times of implantation in a demanding environment. The manufacture of these prior art sockets thus is relatively complicated.

#### Short description of the inventive concept

- 30 According to the invention the molding procedure can be avoided and the design of an interior socket can be simplified to a high degree whilst still meeting the required high standards by designing a pacemaker housing in accordance with the appended main claim. Preferred  
35 embodiments are set forth in the dependent claims.

Short description of the appended drawings

Fig 1 shows a conventional pacer housing with a transparent, molded connective part;

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Fig 2 shows a lead with a male connective part;

Figs 3 - 6 show a preferred embodiment of the connective part in accordance with the present invention;

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Detailed description of preferred embodiments of the invention.

Fig 1 illustrates a conventional pacer housing 1 having a molded, transparent connective part 2. The connective part 2 includes a female socket 3. The inner end of the socket 3 is provided with a longitudinal bore 7 having a relatively small diameter. The bore 7 is provided with a contact surface 4 adjacent to which threads 5 for a set or lock screw are located in a bore 6 oriented orthogonally relative to the female socket. The housing is hermetically sealed also in relation to the molded part 2 and the contact between the interior electronics and the contact surface 4 is achieved by means of a feed-through. The feed-through comprises a ceramic plug, typically made of alumina, into which one or more leads have been soldered. This lead is bonded (e.g. ultrasonically welded) to the electronics and to the contact surface 4. The ceramic plug is soldered or brazed by means of gold into a sleeve made of titanium. This operation may be made at any time before the assembly of the pacer housing. The sleeve is welded into an opening in the housing in a sealing manner during the assembly of the pacer housing that normally consists of two halves. Before the connective part is molded onto the housing, these halves are welded together and sealed.

Fig 2 illustrates a lead 15 comprising a proximal connecting plug 10 and a distal, transvenous, intracardial electrode 16 as well as an attachment means 17 for suturing the proximal end of the lead in the body of the patient. The connecting plug 10 is designed to be received in the socket 3 and the end thereof is provided with a longitudinally projecting contact pin 11 as well as a cylindrical body 17 provided with sealing rings 12, 13, 14 intended to engage and seal against the corresponding inner cylindrical surface of the female socket 3. The shape of the pin 11 corresponds to the shape of the bore 7. When the plug 10 is inserted into the socket 3 the pin 11 engages the contact surface 4 and the set-screw in the bore 6 can be tightened against the pin 11 in order to securely lock the plug 10 in the socket 3. The complexities involved in holding the bores, contact surfaces and threads in position and keeping them open and free from the molding material during the molding process are evident.

For the sake of simplicity, the above prior art device has been illustrated as being unipolar. A bipolar embodiment naturally will be more complex to manufacture. The preferred embodiments of the invention described below will relate to bipolar embodiments.

Figs 3 - 5 show a preferred embodiment of the invention comprising a tubular member 20. For the sake of clarity, the reference signs not repeated throughout all drawings.

The member comprises a tube 21 with two open ends 22, 23. Each end is to be welded into a respective opening in the pacer housing. The tube is made of the same metal as the pacer housing, in this case titanium. The mid-section of the tube is provided with two relatively small lateral openings 24, 25. The openings 24, 25 are sealed by means of a ceramic plug 26 fitting snugly in the tube and soldered with gold against the inside of the tube. Two contact rings 27, 28 have been molded into the ceramic plug overlapping the

lateral openings. The ceramic plug also originally could consist of several separate parts with the contact rings held between and soldered to these parts, thus uniting the parts of the plug to a unitary unit. The soldered junctions then would form an efficient seal.

It should be noted that the size of the openings 24, 25 being necessary to allow the bonding of the leads to the parts of the contact rings accessible through the openings 24, 25 and 31, 32 is small, seen in relation to the entire circumference and to the length of the tube. The openings thus do not affect the structural integrity of the tube. The contact rings 27, 28 moreover overlap the openings and are bonded thereto by means of the intermediate layer of ceramics, in this way strengthening the area in which said openings are located.

Typical dimensions for a tube intended to house a standard IS-1 male connector are for instance an inner diameter of 5 mm, a wall thickness of 0.3 mm (i. e. the same as the thickness of typical pacemaker housing walls) and a diameter of the holes 24, 25 of about 2 mm. A minimum area of about 4 mm<sup>2</sup> is necessary for the equipment presently used for bonding leads to metallic surfaces. The length of the tube is of course adapted to the specific housing into which it is to be placed, but might typically be about 25 mm.

These dimensions of course can be varied as long as the tube remains structurally intact, i. e. as long as the tube has a strength and rigidity that is sufficient to prevent loads, including thermal stresses, on the housing and/or the connector to be transferred as tensile forces to the ceramic parts. Of course, low tensile forces not exceeding the tensile strength of the ceramic could be accepted. Since there are standards regarding the loads a pacemaker housing and connector should be able to withstand and regarding the overall tightness of the housing, variations of the

dimensions only would involve standard stress calculations and dimensioning well within the scope of the man in the art. It should be noted that this also could take the degree of soldering between ceramic plug and tube into account, 5 since this would determine the extent to which tube and ceramic would function as a composite without going outside the ordinary skill of the man skilled in the art.

The ceramic plug is provided with an interior bore 10 corresponding to the shape of the male connector in the same way as the molded prior art female connector described above and thus includes interior sealing surfaces 52, 53 for engagement with the sealing rings on the male connector.

15 A part 30, 31 of the inside of the contact rings is not covered with the ceramic material. In this way two inner circumferential grooves are obtained in the inner bore of the ceramic plug. The bottom of the grooves consists of the metal in the contact rings. Two openings 32, 33 are also 20 provided in the outer surface of the ceramic plug that may be made to coincide with the lateral openings 24, 25 in the tube wall. These openings give access to the contact rings 27, 28 when the ceramic plug has been mounted correctly in the tube 21.

25 Thus, when the ceramic plug 26 has been soldered or bonded into place, the openings 24, 25 will be completely sealed by the plug 26 although allowing electrical connection to the interior of the tube via the contact rings 27, 28.

30 To this extent the tubular member can be manufactured in advance as desired.

Both ends of the prefabricated tube can be welded to the 35 pacemaker housing and the housing parts can be welded together after the connection of interior leads from the interior electronics to the contact rings, should this be desired.

The remaining parts, i. e. the means achieving the contact between the contact rings and the contact surfaces on the male connector part on the lead and the means locking or fixating the male connector part in the socket, can easily  
5 be inserted afterwards. This means for instance that these parts would not interfere with the standard helium-based procedures for testing the housing with connector for leaks or that these parts would not be affected by the leak testing procedure.

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Fig 3 shows the main component parts of the tubular member, the tube 21 with openings 24, 25, the ceramic plug 26, a fixation part 40 and two circular spring contacts 57, 58. The spring contacts are similar to the spring contacts used  
15 in US-A-4,934,366.

The fixation part 40, shown in more detail in Fig 4, is designed in the same way as the lead locking device disclosed in US-A-4,784,141, herewith incorporated by  
20 reference, and comprises a hollow cylindrical part 41 fitting into the end of the tube 21. The inner end of the cylindrical part 41 is provided with an interior flange 42 with an inner conical surface 43. The locking device further comprises a resilient locking ring 44 located adjacent the  
25 flange 42. One side of the ring has a conical surface 45 that is complementary to the conical surface 43. The other side of the ring also has a conical surface 46 that is complementary to a conical surface 47 on a plug 48 provided with exterior threads 49 fitting into interior threads 50 on  
30 the inside of the cylindrical part 41. The outside of the plug 48 is provided with an O-ring 51 that is located in a peripheral groove 52 and sealingly engages the inside of the cylindrical part 41. When the plug 48 is screwed into the cylindrical part 41, the resilient ring 44 will be forced  
35 inwards into contact with the contact pin of the male connector part by means of the interaction of the different

conical surfaces, thus locking the contact pin inside the tube.

The tube 21 preferably is of the same material as the pacer housing, which normally is made of titanium. The ceramic plug may for instance be made of alumina,  $Al_2O_3$ , and the contact rings may for instance be made of stainless steel or of titanium.

10 In the above embodiment the ceramic plug has been illustrated as extending from the end of the tube and past the openings in the side of the tube. It is however only necessary that the ceramic plug cover the openings. The remaining part can be designed as a separate part inserted  
15 and bonded to the tube after the assembly of the pacer housing in a similar way as the fixation means.

Fig 4 shows the tube with all component parts mounted.

20 Fig 5 shows how the tube has been mounted in a pacer housing 60 and welded to openings 61, 62 in the openings via flanges located on the outside of the tube ends. Fig 5 also shows a male connector plug 110 inserted in the tubular member. The plug has a contact pin 111, a contact surface 118 and four  
25 sealing rings 112, 113, 114, 117. The resilient ring 44 grips the pin 111 and the sealing rings 112 - 114, 117 are in engagement with the interior sealing surfaces 52, 53.

The connector means can be achieved in a simple way compared  
30 with the prior art molded connector means.

As mentioned above, the ceramic part can be soldered into the tube in advance by similar methods as used when obtaining the feed-through in the prior art. The tube then  
35 is placed in the openings in one of the pacer housing halves and conductors 55, 56 are bonded (typically by means of ultrasonic welding) to the connecting parts of the



electronic board 54 and to the parts of the contact rings that are accessible via the openings in the tube. The housing halves then are assembled and the two halves and the ends of the tube are welded together by means of a laser beam to form a sealed unit. This unit then is tested for leakage, for instance by means of standard helium-based procedures. It should be noted that no other kinds of work operations than those already used in the prior art are necessary.

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The pacer then is finished by slipping the resilient spring contacts into the respective interior grooves in the ceramic plug and by inserting and bonding the lead locking means into place in the corresponding open end of the tube.

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The new connective part thus is very simple to manufacture and to mount in the pacer housing. The welding and sealing of the housing only includes the additional step of welding the ends of the tube to the edges of the openings in the housing, which is done in the same operation as the welding of the two housing halves. After the welding operation, no further operations are necessary, except for the simple insertion of contact rings and lead locking mechanism.

25 Since the tube after the welding operation in principle forms an integral, load-carrying part of the pacer housing, a high degree of tightness and integrity is obtained. The tube will ensure a high strength and a high durability of the connective part, whilst the ceramic plug will ensure a high degree of tightness in view of the large contact area between ceramic plug and tube that can be used for soldering, i.e. sealing.

Although a pacer housing with one tubular member has been illustrated, the housing of course can contain several members. The housing also wholly or partly could be made of a non-metallic material as long as the parts in which the

openings holding the tube are of metal or of a material allowing a bond of sufficient strength to the metal tube. Furthermore, although the tube has been illustrated as having a circular cross-section, other cross-sections are possible.

One important advantage with the connector according to the invention is that the connecting pin 111 on the end of the lead can be reached from the outside through the end of the tube containing the lead locking means. This will facilitate the removal of the male connector from the female socket since the pin 11 can be pushed outwardly through said second end by means of a tool if the male connector proves to be difficult to pull out. In the above, preferred embodiment it is sufficient to unscrew the threaded plug 48, thus exposing the end of the contact pin 111. Furthermore, in this state a stylet could be introduced into the longitudinal channel, for instance for repositioning the electrode with the aid of the internal electronics in the pacemaker. The plug 48 could also contain a sealable, longitudinal bore, for instance sealed by a screw, for this purpose.

One important feature of the invention is the possibility of achieving a high capacitance between contact ring and tube by allowing the ceramic plug and one of the contact rings to extend all the way to one end of the tube. Ring and tube will be separated by the ceramic, which is chosen to be insulating and thus is a dielectricum. Connecting a small capacitor between ring and tube can increase the capacitance further.

One important advantage of a high capacitance is that it helps avoid interference.